Thermodynamic and Structural Studies on the Human Serum Albumin in the Presence of a Polyoxometalate

D. Ajloo,1 H. Behnam,1 A. A. Saboury,1 F. Mohamadi-Zonoz,2 R. Ranjbar,1 A. A. Moosavi-Movahedi,1 Z. Hasani,1 K. Alizadeh,§ M. Gharanfoli,1 and M. Amani†

Faculty of Chemistry, Damghan University of Basic Science, Damghan, Iran. †E-mail: ajloo@dubs.ac.ir
1Institute of Biochemistry and Biophysics, The University of Tehran, Tehran, Iran
‡Department of Biophysics, Faculty of Basic Science, Tarbiat Modarres University, Tehran, Iran
§Department of Chemistry, Faculty of Basic Science, Tarbiat Modarres University, Tehran, Iran
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Introduction

Albumin is a major plasma protein and binds to the number of drugs altering their pharmacokinetics. It is single chain polypeptide of 585 residues, which comprises about 60% of the plasma protein. It is the major contributor to the oncotic of blood.1 In addition, it has been reported that albumin is chiefly responsible for maintainance of blood pH.2,3 The human serum albumin (HSA) is named a multifunctional plasma carrier protein because of its ability to bind to an unusually broad spectrum of ligands. These includes inorganic cations, organic anions, various drugs, amino acids, and perhaps most important and physiologically available hydrophobic molecules such as bilirubin and fatty acids.1,4,5

In mammals, albumin is synthesized by the liver and possesses a half-life in circulation of 19 days.6,7 Serum albumin has been one of the most studied proteins for 40 years, because its primary structure is very well known for a long time and its tertiary structure was determined a few years ago by X-ray crystallography.5,6 Its primary structure is characterized by low content of tryptophan, a high content of cystein stabilizing a series of main loops, and charged amino acids such as aspartic and glutamic acids, lysine and arginine.2 The apparent repeating structural features, large and small loops and connecting segments, suggest that albumin evolved through a series of gene duplications.3 Its secondary structure is constituted of 67% of helix of six turns and 17 disulfide bridge.5,8 The tertiary structure is composed by three domains I, II, III. Each domain is constituted by a cylinder formed by six helices, and each one of these domains are constituted by two subdomains formed by three helices that covalently linked by their double Cys bridge. These subdomains are IAB, IC, IIAB, IIC, IIIAB, IIIC.5,9

On the other hand, same as all of ligands, several compounds such as polysulfates, polysulfunates, polycarboxylates, polyphosphates and polyoxometalates (POM) have been identified that pharmaceutical effect and inhibit an early stage in the replicative cycle of the human immuno-deficiency virus (HIV).12 Polyoxometalates are early transition metal oxygen anion clusters. More specifically, they are oligomeric aggregates of metal cations (usually the d6 species V(V), Nb(V), Ta(V), Mo(VI), and W(VI) bridged by oxide anions that are formed by self-assembly processes. There are two generic families of POMs, the isopoly and the heteropoly

The interaction of a polyoxometal (POM), K6SiW11Co(H2O)O39.10H2O (K6) as a Keggin, with human serum albumin (HSA) was studied by different methods and techniques. Binding studies show two sets of binding sites for interaction of POM to HSA. Binding analysis and isothermal calorimetry revealed that, the first set of binding site has lower number of bound ligand per mole of protein (ν), lower Hill constant (n), higher binding constant (K), more negative entropy (ΔS) and more electrostatic interaction in comparison to the second set of binding site. In addition, differential scanning calorimetry (DSC) and spectrophotometry data showed that, there are two energetic domains. The first domain is less stable (lower Tm and Cp) which corresponds to the tail segment of HSA and another with more stability is related to the head segment of HSA. Polyoxometalate also decreases the stability of protein as Tm, secondary and tertiary structure as well as quenching of the fluorescence decrease. On other hand, perturbations in tertiary structure are more than secondary structure.

Key Words: Polyoxometalate, Human serum albumin, Isothermal titration calorimetry, Circular dichroism, Fluorescence
compounds. Several general attributes of POMs render them attractive for applications in medicine. The principle advantageous feature of POMs is that nearly every molecular property that impacts the recognition and reactivity of POMs with target biological molecules can be altered. These include polarity, redox potentials, surface charge distribution, shape, and acidity. Polyoxometalates have various molecular and electronic structures with analytical, biological, clinical, geochemical and topological applications. In particular, these compounds have attracted attention in view of their potential application in catalysis and as antiviral and antimutagens. These complexes exhibited biological activity as new potent class of anti-HIV drugs. Interaction of these drugs and their derivatives with biological structures is one of considerable interest, since they have possible medical applications. Two general types of POM activity, antiviral and antimutagenic, have dominated the medicinal chemistry of these compounds to date. The polyoxometalates block the binding of HIV particles to the CD4 cells. They block the binding of recombinant gp120 to SUP-T1 cells in a concentration-dependent manner. They also inhibited the binding of anti-gp120 mAb to HIV-1-infected MT-4 cells. The principal disadvantage of POMs is that they are not organic species. Because low molecular weight organic species dominate in the pharmaceutical industry (drug discovery, synthesis, and development). Increasing the charge and formula weight make enhance the IC50 and EC50.

HSA, (free fatty acid) was obtained from Flucka Chemical Co., and used as received. All of the other chemicals were in analytical grades and purchased from Merck and Sigma chemical Co. The POM and HSA solutions were freshly prepared in all experiments, before spectral analysis. The solutions were prepared with double distilled deionized water. Dialysis bag ultra pure, life technology, 3/4 inch diameter, 14000 Daltons cut-off was purchased from GIBCOBRL Co.

Methods

Isothermal titration microcalorimetry: Enthalpy measurements were carried out with a four-channel commercial microcalorimeter (Thermal activity monitor 2277, Thermometric, Sweden). Every time, 20 μL of 0.5 mM ligand (K6) solution was injected into the calorimetric vessel which contained 2 mL of HSA (1 mg/mL) in 10 mM phosphate buffer (pH 6) by using a Hamilton syringe. The injection of ligand into the perfusion vessel was repeated 20 times. The enthalpy change for each injection was calculated by “Digitam 3” computer program. The enthalpy of dilution of the ligand solutions were measured as described above when the HSA protein was excluded. The enthalpy of dilution for the ligand was subtracted from the enthalpy of protein-ligand interaction. The enthalpy of dilution of HSA is negligible. The molar mass of the HSA protein was taken 66500 Dalton for all calculation.

UV-Vis spectrophotometry: The effect of POM on thermal stability of POM was also investigated by thermal scanning UV-Vis spectrophotometer, Cary 100-Bio model. Variation of absorbance at 280 nm (ΔΔA280) versus temperature (30–90 °C) with 1 K/min scan rate was studied at pH = 6 and 10 mM phosphate buffer. Initial volume of buffer was 600 μL. This experiment carried out in the first for 0.5 mg/mL of HSA in the absence of POM then studied in the presence of 3 × 10−5 M POM in the same condition. Inflection point of above curve ΔΔA280 is Tm or melting point that is a criterion for stability of protein.

Circular dichroism spectroscopy measurements: Circular dichroism measurements were performed with a Jasco J-715 spectropolarimeter. The samples were analyzed in quartz cells with path lengths of 1 mm. Far-UV and near-UV wavelength scans were recorded from 200 to 250 nm and 250 to 320 nm, respectively. All the CD spectra were corrected by subtraction of the background for the spectrum obtained with either buffer alone or buffer containing the ligand. The observed ellipticity in degree (θ) at 280 nm, in degrees cm2 dmol−1. Secondary and tertiary structure of HSA in the absence and presence of 4, 9 and 14 fold concentration of POM investigated in 10 mM phosphate buffer pH 6 and 27 °C. Far-UV CD spectra region was used for the secondary structure and near UV-CD for tertiary structure. Concentration of HSA for secondary and tertiary structures were 0.3 mg/mL and 3 mg/mL respectively. The molar ellipticity was calculated on the basis of the following equation:

\[ [\theta]_d = \frac{100\text{MRW}[\theta]_d}{C \times l} \]
Where $C$, $l$ and MRW are protein concentration in mg/ml, the length of light path in cm and mean amino acid residue weight, respectively.

**Steady-state fluorescence measurements:** Steady-state fluorescence measurements were performed with a Luminescence Spectrometer LS 50B Perkin Elmer at 27 °C. A solution of 0.015 mg/mL HSA was excited at 290 nm in the absence and presence of different volume of $5 \times 10^{-5}$ M POM. The emission spectra were followed at 337 nm. A 10 mm path length quartz cell with a Teflon stopper was used. Care was taken to avoid the presence of significant air pockets. The cuvette was placed in a thermostatically controlled cell holder with a temperature of accuracy ± 0.1 °C.

**Differential scanning calorimetry:** Differential scanning calorimetry of protein was studied by microcalorimeter Scal-1 model with 2 K/min scan rate. High pressure gas was used for prohibiting bubble formation. Thermogram for POM. The emission spectra were followed at 337 nm. A 10 mm path length quartz cell with a Teflon stopper was used. Care was taken to avoid the presence of significant air pockets. The cuvette was placed in a thermostatically controlled cell holder with a temperature of accuracy ± 0.1 °C.

**Dynamic dialysis:** In the first part of the experimental work, 2 mL of 10 mM phosphate buffer solution, pH 6.0, containing of 2.5 mM of $K_6$ was put into a dialysis bag which was placed in 150 mL of buffer solution, in a way that the level of solution of inside and outside the bag became nearly identical. The outside solution was stirred regularly and POM concentration therein was measured every 10 min. In the second part of the experiments, 2 mL of the buffer solution containing 2 mg/mL of protein was put into a bag. $K_6$ concentration outside the dialysis tubing was measured as above.

For the standard curve, solutions of $K_6$ with concentrations in the range of $0-2 \times 10^{-5}$ M were prepared in the phosphate buffer and their absorption were determined at 250 nm.

**Results and Discussion**

There are several methods for ligand binding investigations.19-26 Equilibrium dialysis is one of the most general methods for this purpose. A disadvantage of this method is being relatively time consuming and demanding for higher concentration of the sample in the experiment. On the other hand, the dynamic dialysis method is relatively more precise, faster and requires less sample than equilibrium dialysis. The most important point is that, there is no absorbance interference in this method. Some of ligands and macromolecules may have absorbance interference in the studied wavelength. In this work, POM and HSA have a maximum absorbance at about 250 nm and 280 nm wavelengths, respectively. Thus, to prohibit any absorbance interference in our studies, we have used the dynamic dialysis method. To obtain binding parameters, one needs to evaluate the number of bound ligands to protein. Therefore, we present some of necessary equations for this purpose.21 The first Fick’s law states that:

$$J = -D\frac{dC}{dx} \quad (2)$$

Where, $J$ is flux, $D$ is the diffusion coefficient and $dC/dx$ is the gradient of concentration. Given in the experiments the volumes of the solutions inside and outside the bag are actually fixed, finite and stirred, thus:

$$\frac{\Delta C}{\Delta x} = \frac{C_i - C_o}{d} \quad (3)$$

and

$$J_{i \rightarrow o} = \frac{1}{A} \cdot \frac{dn}{dt} = -D \frac{C_i - C_o}{d} \quad (4)$$

Where: $d$ is the constant thickness of the membrane, $n$ is the number of moles of ligand, $C_i$ and $C_o$ are the concentrations of ligand inside and outside, respectively, and $A$ is a constant.

Under the above conditions:

$$\frac{dn}{dt} = \frac{dC_i}{dt} = \frac{dC_o}{dt} \quad (5)$$

and

$$\frac{dC_o}{dt} = k(C_i - C_o) \quad (6)$$

Where $k$ is a constant.

The equation (6) indicates that the variation of $dC_o/dt$ with $\Delta C = C_i - C_o$ should be linear. The values of $dC_o/dt$ can be determined at different times. $C_i$ can also be determined in the absence of the protein, thus $\Delta C = C_i - C_o$ is evaluated. The adsorption by membrane itself is neglected.

Although the equation (6) is not linear in practice, it can be used to construct a calibration curve, from which the

![Figure 1](image-url)
the whole procedure is repeated and the rates, 

\[ \frac{\Delta C}{\Delta t} = \frac{C_i - C_o}{t} \]

The method was used to study the binding of K6 to HSA. In the presence of the protein are obtained. For protein solution we determine the calibration curve, that is, when attaining equilibrium is faster than the rate of diffusion, the corresponding concentrations of the ligand inside the bag, the calibration curve, i.e., a plot of \( \frac{dC_o}{dt} \) versus \( \Delta C = C_i - C_o \), is obtained (cf. Fig. 2). In the presence of the protein the whole procedure is repeated and the rates, \( \frac{dC_o}{dt} \) determined. Then for the same time intervals the corresponding values of \( \frac{dC_o}{dt} \) and \( C_o \) are selected and by the use of the calibration curve, (It is obvious that, when attaining equilibrium is faster than the rate of diffusion, the calibration curve could be used) the \( \Delta C \) and \( C_i \) values in the presence of the protein are obtained. For protein solution we write:

\[ \frac{dC_o}{dt} = k(C_i - C_o) \]  

The method was used to study the binding of K6 to HSA. Figure 1 shows the variation of \( C_o \) against time in the absence and presence of HSA at 27 and 37 °C.

Values of \( \frac{dC_o}{dt} \) corresponding to different values of \( C_i - C_o \) at specified times were obtained and hence the calibration curve, that is \( C_i - C_o \) versus \( \frac{dC_o}{dt} \), was obtained (cf. Fig. 2).

The value of \( k \) depends on the size, surface of dialysis bag and diffusion of samples. In this experiment we compared the diffusion of POM in the absence and presence of HSA. Therefore, if all of the conditions become similar, the \( k \) values are equal. Therefore by elimination of \( k \) in two above equations, we obtain following equation:

\[ C_i' = C_o' + \left( C_i - C_o \right) \frac{dC_o'}{dt} / \frac{dC_o}{dt} \]  

Then average number of ligand bound to the macromolecule, \( \nu \), can be estimated using the following equation:

\[ \nu = \frac{C_i' - C_o'}{C_p} \]  

Where \( C_o \) and \( C_o' \) are total concentration of the protein and initial concentration of the ligand, respectively, and \( C_i' \) was defined earlier and obtained by equation (8). Calorimetric and binding data has shown that we have two sets of binding sites. Thus, applying the Hill equation for two sets of binding sites, we can obtain thermodynamic parameters:

\[ \nu = \frac{g_1(K_1C_i')^{n_1}}{1 + (K_1C_i')^{n_1}} + \frac{g_2(K_2C_i')^{n_2}}{1 + (K_2C_i')^{n_2}} \]  

In this equation, \( g_1, K_1 \) and \( n_1 \) are the maximum number of bound ligand, equilibrium constant and Hill constant for the first set of binding sites, respectively, and \( g_2, K_2 \) and \( n_2 \) are cited parameters for the second set of binding sites. These thermodynamic parameters were estimated by fitting of above equation to experimental data by Sigmaplot 2000.

The results were tabulated in Table 1. This table shows that the binding constant in the first binding set is higher than that of the second binding set. Maximum number of bound ligand (\( g \)) is higher than first binding site. Because in the first step, POM binds to the positive charge on the protein and then unfolding of HSA occurs predominately after saturation of binding sites and then more binding sites become accessible to solvent and ligand.

Hill coefficient (\( n \)) shows the cooperativity of ligand binding process. It reveals that binding of POM facilitates the binding of next ligand. Also the Table 1 shows the effect of temperature on the binding parameters. Increase in temperature, make \( n_1, n_2 \) increase and decreases \( K_1, K_2, g_1 \) and \( g_2 \). It seems that complexation decreases as temperature increases. Because ligand binding is mostly exothermic.

In addition, total enthalpy of binding in each set of binding

<table>
<thead>
<tr>
<th>( t ) / °C</th>
<th>( K_1 \times 10^{-3} )</th>
<th>( K_2 \times 10^{-3} )</th>
<th>( n_1 )</th>
<th>( n_2 )</th>
<th>( g_1 )</th>
<th>( g_2 )</th>
<th>( \Delta H_0^\nu (1) )</th>
<th>( \Delta H_0^\nu (2) )</th>
<th>( \Delta S_0^\nu (1) )</th>
<th>( \Delta S_0^\nu (2) )</th>
</tr>
</thead>
<tbody>
<tr>
<td>27</td>
<td>2.69 (±0.14)</td>
<td>0.27 (±0.01)</td>
<td>1.53 (±0.09)</td>
<td>4.5 (±0.43)</td>
<td>5.5 (±0.2)</td>
<td>10.5 (±0.5)</td>
<td>-40.655</td>
<td>-12.397</td>
<td>-31.57</td>
<td>43.51</td>
</tr>
<tr>
<td>37</td>
<td>1.59 (±0.09)</td>
<td>0.23 (±0.02)</td>
<td>1.43 (±0.16)</td>
<td>5.71 (±0.50)</td>
<td>4.0 (±0.2)</td>
<td>7.6 (±0.3)</td>
<td>---</td>
<td>---</td>
<td>---</td>
<td>---</td>
</tr>
</tbody>
</table>
site, $\Delta H^o_b$, can be estimated using $K$ values in two temperature and van’t Hoff equation:

$$
\ln \left( \frac{K_2}{K_1} \right) = -\frac{\Delta H^o_b}{R} \left( \frac{1}{T_2} - \frac{1}{T_1} \right)
$$

(11)

Using following equation we can also obtain the entropy change of binding process.

$$
\Delta G^o_b = \Delta H^o_b - T \Delta S^o_b
$$

The results are tabulated in Table 1. $\Delta H^o_b$ (1) for the first set is more negative than that for the second set. The number of positive group for the first set may be higher than second set and so electrostatic interaction and exothermicity become higher. $\Delta S^o_b$ is negative and positive for the first and second set, respectively, since the number of free molecules decreases, as ligand binding occurs. Therefore the entropy, which depends on the number of these free molecules, will diminish. Sometimes, ligand binding process is accompanied with unfolding. In this case, some of connections are disrupted and mobility of atoms and residues are increased. Thus the entropy in the unfolded state is higher than that in more compacted form.

In addition, fluorescence spectroscopy was used to monitor changes on the tertiary structure induced by the interaction with ionic POM. These interactions can, in principle, produce changes in the position or orientation of the tryptophan residues, altering their exposure to solvent and leading to an alteration in the quantum yield. Titration of HSA solutions in phosphate buffer at pH 6.0 with POM were performed by adding aliquots of POM stock solution directly to the cuvette and the fluorescence emission spectra were registered. The study of conformational and functional changes of HSA after interaction with POM by fluorescence showed two phenomena. The first is the reduction of fluorescence intensity and the second is a shift in $\lambda$ at maximum intensity ($\lambda_{\text{max}}$) of emission toward lower wavelength. This implies that conformational changes have occurred.

It is also reported that, the Trp 214 is conserved in mammalian albumins and play an important structural role in the formation of the IIA binding site by limiting the solvent accessibility. In addition, it participates in additional hydrophobic packing interaction between IIA and IIIA interface. This is the reason that HSA takes the heart shape.

Figure 3 shows the variation of fluorescence spectrum in the presence of different concentrations of POM. It is observed that a quenching of fluorescence occurs by POM. Alteration of $\lambda_{\text{max}}$ and fluorescence intensity (%F) at $\lambda_{\text{max}}$ were obtained from the Figure 3 and plotted against [POM]/[HSA] ratio which is depicted in Figure 4.

When Trp is rigid and shielded against interaction with other molecules, then the energy transfer and following quenching is low. Increasing the interaction of Trp with other molecules such as, solvent and ligand molecules, make increases the energy transfer from Trp to other molecules and the intensity increases (increases quenching).

Figure 4 also shows the comparison of calorimetry and fluorescence results. It is significant to note to the similar trend in the calorimetry and fluorescence data. Calorimetry data shows that ligand binds to HSA electrostatically in the first. The exothermic interactions (mostly electrostatic) correspond to decreasing part of heat curve. Thus the injection of more ligands releases the heat. This released heat due to binding, causes dissociation of some of connections (except covalence bond) and results in unfolding of protein. Therefore, this later process is endothermic. We see two minima in calorimetry and fluorescence curves which are related to presence of two structural domains for binding. Because, the X-ray crystallographic data and the three-dimensional struc-

Figure 3. Emission spectra of HSA (0.03 mg/mL) in 10 mM phosphate buffer at pH = 6 and 27 oC. Excitation carried out at 290 nm in different ratio of [POM]/[HSA] same as Figure 4. The arrow in the figure shows that, the increasing the POM concentration is accompanied with decreasing the fluorescence intensity. The lowest spectrum corresponds to the highest concentration of POM.

Figure 4. Heat of interaction of POM with HSA (up) and fluorescence intensity as well as $\lambda_{\text{max}}$ (down) in different ratio of [POM]/[HSA] and 10 mM phosphate buffer at pH = 6 and 27 oC.
Thermodynamic and Structural Studies on the Human Serum Albumin


ture of HSA showed two distinct segments.7,31 One extra compacted segment as the head of HSA molecule, which is the result of intermolecular interactions of IA, IB and IIA subdomains. Whereas another segment, tail of the molecule, is more extended than the head part and contains IIB, IIIA and IIIB subdomains. The stability of the tail is less than the head part and has a loose conformation when compared to the head region.7,31

Thus, two minima in the Figure 4 are probably related to bindings to the cited domains. First (A and B steps) and second (C and D steps) minima correspond to interaction of ligand to more and less accessible domain, respectively. The A and C sections are related to an increase in exothermicity, while B and D correspond to a decrease in exothermicity (increase in endothermicity due to unfolding). Because unfolding process is the endothermic process. On the other hand, rate of quenching (curvature of %F curve) in A and C is higher than that in B and D. λ_{max} goes to lower wavelength in A and C and to higher wavelength than that in B and D. The cause of these observation is that the interaction of POM with HSA makes increasing the energy transfer (quenching) due to proximity of Trp or other fluorophores to ligand and solvent molecules following increasing its flexibility and accessibility. When the electrostatic interaction goes to minimum or saturates the opposite charge by POM, then repulsion between the negative charge of ligand and π electrons of aromatic ring lead the fluorofore to a region of less polarity (λ_{max} goes to higher wavelength at B and D).

Thus, A and C steps correspond to a decrease in endothermicity, ΔH and %F, whereas C and D steps are related to an increase in endothermicity, λ_{max} and slow decrease in %F.

Figure 5 shows the variation of C_{p, excess} of HSA versus temperatures when incubated with POM. The reversibility of the thermal denaturation of the samples up to 80 °C was assayed by rescanning after cooling the sample that was previously scanned thermally. Also, Figure 6 contains the deconvolution results of thermal profile. Deconvolution of excess heat capacity into sequential two-state transitions was carried out in upward direction by utilization of Scal-2 software. The resulting deconvolution parameters were optimized by fitting program of the related software. The calculated fitting error was less than 0.015 that represent energetic domains with special T_m and enthalpy of unfolding (ΔH_m). The thermal denaturation profile of HSA in the absence of POM was reversible up to 75 °C (data not shown). Therefore the denatured line was not accessible and it is impossible to obtain the deconvolution profile for HSA in the absence of POM.12

DSC data shows that, there are two energetic domains in thermal profile. One of them, has lower T_m and ΔH (313 K and 136 kJ/mol) that may be related to unfolding of weak binding or tail of HSA and the other with higher T_m and ΔH (338 K and 141 kJ/mol) is related to more compact domain and stronger parts of molecule (head of HSA).

Figure 6 shows the effect of different concentration of K_6 on the secondary and tertiary structure of HSA. The values of different parts of CD were tabulated in Table 2. POM reduces the secondary and tertiary structure. The results show that the tertiary structure has changed relatively more than the secondary structure. It shows that α-helix decreases, β-structure increases and random coil variation are not regular. Last column of this table also shows fluorescence.

![Figure 5](image1)

**Figure 5.** Thermogram of human serum albumin (HSA) in the presence of 0.045 mM of POM in 10 mM phosphate buffer. Subpeaks were obtained by deconvolution of C_{p, excess} profile.

![Figure 6](image2)

**Figure 6.** Near and far (inset of figure) UV circular dichroism spectra of the HSA protein. CD spectra were recorded for the HSA protein in the absence (a) and presence of (b) 4 (c) 9 d (14) molar ratio of [POM]/[HSA]. The HSA concentration was 0.3 mg/mL and 3.0 mg/mL for far and near UV-CD, respectively.

<p>| Table 2. The effect of POM on the secondary structure and fluorescence intensity at pH = 6 and 27 °C |</p>
<table>
<thead>
<tr>
<th>[K_6]/[HSA]</th>
<th>Alpha Helix %</th>
<th>Beta Structure %</th>
<th>Random%</th>
<th>%F</th>
</tr>
</thead>
<tbody>
<tr>
<td>0</td>
<td>30.4</td>
<td>41.0</td>
<td>28.6</td>
<td>81.1</td>
</tr>
<tr>
<td>4</td>
<td>29.9</td>
<td>41.6</td>
<td>28.5</td>
<td>37.4</td>
</tr>
<tr>
<td>9</td>
<td>29.5</td>
<td>43.2</td>
<td>27.2</td>
<td>27.8</td>
</tr>
<tr>
<td>14</td>
<td>29.3</td>
<td>42.2</td>
<td>28.4</td>
<td>23.2</td>
</tr>
</tbody>
</table>
Intensity (%F) in the same ratio for comparison of structural changes in two methods.

On the other hand, midpoint of thermal transition ($T_m$), as a parameter for comparison of the thermal stability, obtained from Figure 7. It shows percent of variations at 280 nm (% $\Delta A_{280}$) for determination of $T_m$. It can be obtained from derivation of the curve of Figure 7. As we see, POM decreases the $T_m$ of protein from 78 to 73°C. Thus POM destabilizes the HSA.

### Conclusion

Ligand binding process often associates with denaturation of macromolecules (folding or unfolding). Some of them are exothermic (such as electrostatic interaction) and others are endothermic (such as unfolding). Thus, the primary interactions are usually electrostatic. Heat of exothermic process supports the unfolding process. Therefore the required heat for unfolding is often obtained from exothermic interactions. Downward trend of heat curve is related to exothermic (mostly electrostatic) and upward trend of curve is related to endothermic (mostly unfolding) process. Variations of calorimetry and fluorescence data show a common fact. Their curves have two minima. First minimum corresponds to interaction with more exposed positive amino acids and less stable domain (lower $T_m$ and $C_p$ in DSC and UV experiments) and the second minimum is related to less exposed positive amino acid and more stable domain. Entropy change in the first set is negative whereas in the second site is positive. Interaction with the first set in here is more favorable because it has higher binding constant ($K$) and it is prior to the second. The first set is thermodynamically less stable. Thus we can ascribe it to the tail of HSA and more stable domain relates to head of HSA. Also POM ligand destabilizes the protein structure.

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### References