Effect of Fatigue on Force-Matching in the Quadriceps Muscle

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Abstract

This study examined the ability of human subjects to match a force in their quadriceps muscle during fatigue. Twenty subjects (mean age: 23.4 yrs, mean height: 167.8 cm, mean weight, 62.6 kg) were enrolled in the experiment. In the force-matching task, the quadriceps muscle generated 50% of the MVIC (maximum voluntary isometric contraction) torque under visual control and then without visual feedback. After inducing fatigue in the quadriceps muscle, the subjects were required to match 50% of the MVIC torque without visual feedback. The perceived magnitude of the force and force-matching errors were measured. 50% of the MVIC torque was perceived from 39.96 Nm in the pre-fatigue condition to 44.95 Nm in the post-fatigue condition. 50% of the MVIC torque matching errors increased significantly from .55% in the pre-fatigue condition to 9.6% in the post-fatigue condition (p<.001). In addition, there were significantly more force-matching errors in women than in men (p<.01). In conclusion muscle fatigue can interfere with a subject’s ability to match a force. This suggests that muscle fatigue may contributes to the sensitization of the proprioception.

Key Words: Fatigue; Force-matching; Proprioception.

Introduction

Recently, researchers have widely assumed that joint proprioception plays an important role in maintaining the functional stability of a joint (Swaink et al, 2001; Tsuda et al, 2001). Proprioception is defined as the cumulative neural input to the central nervous system from specialized nerve endings known as mechanoreceptors (Lee et al, 2003). It is a specialized variation of the sensory modality of touch and encompasses the sensation of the joint motion and joint position (Grigg, 1993). The sensory receptors for proprioception are located in the skin, muscles, tendons, and joint capsule as well as in the ligaments. Mechanoreceptors function as transducers that convert a mechanical load in the joint to afferent impulses. This information is finally integrated for the motor programming required for precision movements and contributes to reflex muscle contraction, providing dynamic joint stability. Miura et al (2004) reported that muscle fatigue has been shown to adversely alters joint proprioception and impairs neuromuscular control in the lower extremities. Muscle fatigue is a complex phenomenon that has been defined as a decrease in the force-generating capacity regardless of the task performed. Muscular fatigue is an inevitable phenomenon in physical and daily activities (Vuillerme et al, 2002). Therefore, deterioration in proprioception as a result of physical or mental fatigue may increase the risk of knee ligamentous injuries. For example, the incidence of injury to skiers and football players is higher in the afternoon (Tuggy and Ong, 2000) and the third quarter, respectively (Zempher, 1989). This suggests

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that fatigue in athletes might produce a decrease in knee proprioception and is one of the risk factors for knee ligament injury.

Limb position or muscle force-matching task are used to measure the reduced proprioception during a fatiguing contraction. The sense of force is complicated in that it actually incorporates two senses, a peripherally derived sense of force and a centrally derived sense of effort (McCloskey et al, 1983). The sense of force is mediated by the skin and joint or muscle afferent fibers. In particular, the Golgi tendon organ detects the original muscle force (Gandevia and Burke, 1992). It has also been proposed that the Ia muscle spindle afferents are capable of signalling the intramuscular tension (Cafarelli, 1988).

McCloskey et al (1974) suggested a contralateral limb matching method to match force. In this method, the participants are required to generate a specified level of force by contracting the muscles of the reference limb in the presence of external feedback, and then to match the subjective magnitude of this force, using the muscles of the contralateral matching limb without the assistance of feedback. The individuals were required to reproduce a force applied during sustained fatiguing isometric contractions, by generating a brief matching contraction using the contralateral limb.

Generally, there is a monotonic increase in the perceived magnitude of the reference force when subjects are required to reproduce a force (Cafarelli and Layton-Wood, 1986; Gandevia and McCloskey, 1978; Jones and Hunter, 1983a, 1983b). Therefore, any decrease in force-generating capacity due to fatigue should therefore be perceived as a proportional increase in effort. Weerakkody et al (2003) proposed that fatigue altered the relationship between sense of effort creating a the sense of tension. However, Carson et al (2002) suggested that the motor command is associated with the sense of effort. The mechanism of force matching errors by a monotonic increase in the perceived magnitude of force is controversial.

This study examined the relationship between the perceived magnitude of force and the force matching errors after the quadriceps muscle was fatigued. Therefore, it was assumed that fatigue would affect the sensitization of proprioception.

Methods

Subjects

A total of 20 subjects (10 males, and 10 females) were enrolled in this study. The subjects were required to have no existing musculoskeletal abnormalities, or be involved in any regular leg resistance exercise programs. All the subjects provided informed consent after being explained the purpose and method of the study. The mean age, was 23.4 years, and height 167.8 cm, weight 62.6 kg (Table 1).

Table 1. Subjects characteristics

<table>
<thead>
<tr>
<th></th>
<th>Male (n=10)</th>
<th>Female (n=10)</th>
<th>Total (N=20)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age (yrs)</td>
<td>23.8±3.2*</td>
<td>23.1±4.7</td>
<td>23.4±3.9</td>
</tr>
<tr>
<td>Height (cm)</td>
<td>173.5±3.6</td>
<td>162.1±4.8</td>
<td>167.8±7.2</td>
</tr>
<tr>
<td>Weight (kg)</td>
<td>71.8±8.7</td>
<td>53.5±4.3</td>
<td>62.6±11.5</td>
</tr>
</tbody>
</table>

*Mean±SD.

Equipment

Torque sensor

A torque sensor was connected with an N-K table along the axis of rotation coincident with the knee joint. The subjects were comfortably seated with their trunk and their leg and ankle were strapped by a belt and they were able to grip both handles. The torque sensor was fixed with 110° to generate the maximum voluntary isometric contraction (MVIC) in the quadriceps muscle. The torque traces were acquired using Acqknowledge.
37.3 software for the subsequent analysis. The sampling rate in the torque sensor was 100 Hz.

**Procedures**

**Pre-fatigue testing**

The participants extended their knee joints to maximum extension for 5 seconds with the knee joint 70° in order to estimate the maximum voluntary isometric contraction (MVIC) torque in their quadriceps muscle. Three MVICs of 5 seconds duration were carried out and averaged. This value was taken as the MVIC. The target torque was 50% of the MVIC torque (the range 45~55% of the MVIC). The subjects were able to see a computer monitor that provided visual feedback of the torque level generated by the quadriceps muscle. They were asked to generate 50% of the MVIC torque under visual control. Once the subjects had satisfactorily achieved 50% of the MVIC torque, they were asked to match it without displaying the torque output. The subjects were instructed to say "now" when they believed 50% of the MVIC torque in the leg had been matched, at which point the level was recorded. A verbal cue to correct the level of torque was used. Three force matching sessions of 5 seconds duration were carried out and the results were averaged. This value was taken as the force-matching errors.

**Induced fatigue**

The participants extended maximally with knee joint 90° to the maximum extension to estimate the MVIC in their quadriceps muscle. They maintained 80±5% of the MVIC torque under visual feedback until they could not last for more than 10 seconds.

**Post-fatigue testing**

After inducing fatigue in the quadriceps muscle, the torque sensor angle was changed to 70°. The subjects were asked to generate 50% of the MVIC torque under visual control again. And then they were required to match 50% of the MVIC torque without displaying a torque output. Three force matching sessions of 5 seconds duration were carried out and the value greater than 45~55% of the MVIC torque was averaged. This value was taken as the force-matching error.

**Statistical Analysis**

A paired sample t-test was performed to test the significance in 50% of the MVIC torque matching errors produced by the quadriceps muscle. The collected materials were coded and analyzed by SPSS version 12.0 for Windows.

**Results**

**The perceived magnitude of 50% of the MVIC torque**

50% of the MVIC torque was perceived to be 39.96 Nm in pre-fatigue and 44.95 Nm in post-fatigue (Table 2).

**50% of the MVIC torque-matching errors**

50% of the MVIC torque matching errors were significantly increased from 45% in the pre-fatigue state to 9.6% in the post-fatigue state (p<.001) (Table 3). In addition, the force matching errors were significantly higher in women than in men (p<.01) (Table 3).

**Table 2. Changes in the perceived magnitude 50% of the MVIC torque**

(Unit: Nm)

<table>
<thead>
<tr>
<th></th>
<th>MVIC 45~55%</th>
<th>The perceived 50% of the MVIC torque</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Pre-fatigue</td>
<td>Post-fatigue</td>
</tr>
<tr>
<td>Male (n1=10)</td>
<td>45.78~55.96</td>
<td>52.79</td>
</tr>
<tr>
<td>Female (n2=10)</td>
<td>23.59~28.84</td>
<td>27.14</td>
</tr>
<tr>
<td>Total (N=20)</td>
<td>34.69~42.40</td>
<td>39.96</td>
</tr>
</tbody>
</table>
Table 3. Changes in 50% of the MVIC torque matching errors (Unit: %)

<table>
<thead>
<tr>
<th></th>
<th>Pre-fatigue</th>
<th>Post-fatigue</th>
<th>t</th>
<th>p</th>
</tr>
</thead>
<tbody>
<tr>
<td>Male (n=10)</td>
<td>0</td>
<td>5</td>
<td>-2.014</td>
<td>0.037</td>
</tr>
<tr>
<td>Female (n=10)</td>
<td>1</td>
<td>14*</td>
<td>-6.406</td>
<td>0.000</td>
</tr>
<tr>
<td>Total (N=20)</td>
<td>55</td>
<td>9.6</td>
<td>-4.933</td>
<td>0.000</td>
</tr>
</tbody>
</table>

*Significant difference in post-fatigue between male and female.

Discussion

It is essential that the sense of joint position should be detected in order to control muscle and have precise timing. Muscle fatigue can produce the disturbances in the proprioception, changes in the perception of the muscle and limb position and movement, which can generate errors in the tracking force and limb position after exercise (Brockett et al., 1997). Vuillerme et al. (2002) reported that subjects sway more under fatigue conditions than in the non-fatigue conditions as indexed by the increased range, mean speed, and dispersion of COP displacements with fatigue. Skinner et al. (1986) reported a decrease in knee proprioception, with a 15% decrease in knee flexion and extension work output after a general fatigue load. Miura et al. (2004) reported that a general fatigue load had a statistically significant effect on knee proprioception.

This might be a central processing deficiency in the proprioception signal by the central fatigue process. Central fatigue reduces accuracy in motor control and disturbs the voluntary muscle stability activity to endure stress loading at the joint. Finally, it increases the risk of ligament injury at the knee joint.

This study showed that 50% of the MVIC torque matching errors were increased significantly from 5.5% in the pre-fatigue condition to 9.6% in the post-fatigue condition. Force matching errors in women were increased significantly from 1% in the pre-fatigue condition to 14% in the post-fatigue condition. In men, the force matching errors increased significantly from 0% in the pre-fatigue condition to 5% in the post-fatigue condition. The force matching errors were significantly higher in women than in men. This suggests that the perceived forces for the required force in magnitude were either increased or decreased by muscle fatigue. 50% of the MVIC torque perceived in women was 27.14 Nm in the pre-fatigue condition and 32.67 Nm in the post-fatigue condition. In men, the perceived forces increased from 32.79 Nm to 57.22 Nm in the pre- and post-fatigue condition. Stevens and Cain (1970) reported that when subjects are asked to evaluate the magnitude of the force exerted by fatigued muscles, there was a uniform ratio increase in the perceived amplitude of the forces. Teghtsoonian et al. (1977) reported that muscle fatigue was associated with a substantial change in the exponent of the force power function, and the absolute threshold for detecting a force might increase with increasing muscle fatigue. An the normal circumstances, the motor command provides a reasonable representation of the sense of effort. However, after tensile exercise, when the contractile elements are disturbed by muscle fatigue, there are several fatigue-related mechanisms involved at different levels of the nervous system that can affect the regulation of these small forces. At the peripheral level, pre- and post-synaptic mechanisms and sites are potentially implicated, which include a failure in the transmission of the neural signal or a failure of the muscle to respond to neural excitation (Bigland-Ritchie and Woods, 1984). In the central system level, to maintain constant force level, the motor cortex increases a complex series of excitability and produces more efforts in order to maintain a constant force (Carson et al., 2002; Jones, 1995).

Prosko et al. (2004) suggested that after a series of eccentric contractions there are large force matching
errors due to three causes. First, there was greater effort required to achieve a given force, as a result of fatigue and muscle damage. Second, there is an increase in the central neural drive, presumably accompanied by an increase in effort, which lasts for up to 48 hours. Third, there is the influence of DOMS (delayed onset muscle soreness), which does not begin to exert a significant effect until 24 hours after the exercise, and which lasts for at least four days.

It is not known if the frequent failure in exercise performance due to muscle fatigue is due to impaired proprioception or to other factors. However, there is some evidence that the output of the muscle receptors changes in fatigue (Christakos and Windhorst, 1986). In addition, stretch reflexes, which can indirectly reflect the output of proprioceptors, have been reported to increase (Hakkinen and Komi, 1983), decrease (Balestra et al., 1992), or remain unchanged (Darling and Hayes, 1983).

The aim of this study was to test the perceived magnitude of force and force-matching errors, as well as to demonstrate that proprioception is sensitized by muscle fatigue. The sense changes related to maintaining a constant force was examined in order to determine the perceived magnitude of force constantly at various times. However, further study will be needed to determine the different joint levels associated with the force level associated with force-length relationship. In addition, a training programme through force matching is recommended for patients with a musculoskeletal injury.

**Conclusion**

This study examined the ability of human subjects to match a force in their quadriceps muscle during fatigue. The perceived 50% MVC torque was 39.96 Nm in the pre-fatigue condition and 44.95 Nm in the post-fatigue condition. 50% of the MVC torque matching errors increased significantly from 55% in the pre-fatigue condition to 9.6% in the post-fatigue condition (p<0.01). There were larger force-matching errors in women than in men (p<0.01). In conclusion, muscle fatigue can interfere with a subject’s ability to match a force. This suggests that muscle fatigue can contribute to the sensitization of proprioception.

**References**


Stevens JC, Cain WS. Effort in isometric muscular contractions related to force level and duration. Percept Psychophys. 1970;8:240-244.


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